

09/936169

2/PATS

TITLE

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Self-tapping implant

TECHNICAL FIELD

10 The present invention relates to a self-tapping
implant for bone, preferably jawbone. The implant
comprises a body with threads arranged thereon, and a
conically tapering portion arranged at its front end.
In addition, there are one or more spaces, here called
15 bone-chip recesses, which accommodate bone material cut
off during tapping and which are formed by removal of
material from the threads and body in question. Each
materially reduced thread has a cutting edge which
extends inwards from the outer edge of the respective
20 remaining part and which cooperates with the
bone/jawbone during tapping.

PRIOR ART

25 Self-tapping dental implants are already well
known. A characteristic of many implant types is that
they have a relatively dense threading. There are also
implants with relatively sparse threading. It is also
known to provide implants with multiple threads, for
30 example double threads, by which means the speed of
screwing can be increased. In principle, the thread
configurations used aim to make it easier to screw the
implants into jawbone or other bone in the human body,
and to provide initial anchoring of the implant in the
35 bone. Reference is made, inter alia, to Swedish Patent
9601913-8, which discloses an implant with a conically
tapering front end and with spaces or bone-chip
recesses provided for bone material that has been cut
off. Reference is also made to EP 0 641 549 which shows

that it is already known per se to use multiple threads on implants.

DESCRIPTION OF THE INVENTION

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TECHNICAL PROBLEM

There is a general need to provide good cutting characteristics on the implant so that the latter can be fitted without preliminary threading, which means, among other things, that the implant has to be designed with a thread-cutting point which is formed with a special cutting geometry. The invention aims to solve this problem among others.

In connection with the design of the implant, the aim is to avoid using a dense threading, as this entails a low insertion speed. Nor is a sparse threading wanted, as this entails small thread surfaces in contact with the bone tissue and, consequently, poor conditions for successful osseointegration. If the thread is given a deep profile, it is possible to compensate for this, but at the expense of the implant's strength. The use of double threads is not completely free of problems either in this context, since a double thread, at each moment of insertion, must cut away twice as much bone, which means that the double-threaded implant meets considerably greater resistance from the bone. Theoretically, the cutting resistance is approximately twice as great. During insertion, frictional forces also have the effect that the total resistance can be about 50% higher compared to the case of a corresponding implant geometry with a single thread. For this reason, double-threaded implants are advantageously used mainly in soft bone. The use of double-threaded implants in hard bone entails high insertion resistance from the bone. An implant can always be fitted using a thread tap, but a double-threaded design does not then represent any simplification or saving in time. The present invention also solves this problem and discloses a novel approach

in which the implant is provided with excellent cutting characteristics which mean that it can be fitted without preliminary threading in the bone or jawbone in question.

5 In these types of implants, there is a further requirement that the implant must be designed with sufficient strength. This is especially important in hard bone, where the resistance to the screwing-in function can be considerable. The need for considerable
10 or sufficient strength is often in conflict with the need for a suitable cutting geometry or thread design. The invention solves this problem too.

SOLUTION

15 The novel approach disclosed by the invention entails, inter alia, that the thread-cutting point of the implant is designed with a special cutting geometry which in embodiments is combined with features known
20 per se, and these, taken together, afford an especially advantageous threading function for the self-tapping implant.

 The feature which can principally be regarded as characterizing an implant according to the invention
25 is that each cutting edge of a number, preferably all, of the cutting edges of the removed threads have a pointed shape which, in the cross section of the thread in question, essentially follows a line which deviates from a radius through the remaining thread part's front
30 portion or the pointed shape's point. The cutting angle or chip angle formed by the pointed shape is chosen so as to give an effective threading property which is in relation to the threading property of the implant, i.e. ensures sufficient remaining materially-reduced thread
35 and body. The relationship between cutting properties and strength is preferably optimal.

 In a preferred embodiment, the cutting angle or chip angle is about 20° and is chosen preferably within a range of 15-40°. The said refinements can also

include the cutting edge on a first remaining thread part merging via a radius or curved part into a rear edge on a second remaining thread part, which lies before the first thread part in the direction of screwing of the implant. The radius or the curved part is in this case arranged to provide optimum remaining material in the body and remaining thread part or thread parts and, consequently, optimum strength of the implant in question.

10 The conically tapering portion or tip of the implant must be arranged to support at least two thread parts which extend out to the full radial dimension of the thread in question. The point angle of the cone-shaped portion or cone-shaped implant tip is preferably less than about 20° . A thread relief which is to be effected by removed or materially reduced thread parts is preferably arranged on the conically tapering portion or the point in order to reduce or minimize clamping tendencies between the implant and the bone tissue during threading. The bone chip cutting edge is also preferably arranged non-axially. One or more remaining thread parts on one or more threads are provided with material reduction behind, as viewed in the direction of screwing, the full diameter part which can be engaged with the bone or the bone tissue, for the purpose of facilitating the relief function upon threading.

ADVANTAGES

30 By means of what has been proposed above, an excellent screwing function is obtained for implants in dentine or other bone types. The design of the specific cutting edges and the remaining thread part and the connection of this to the body guarantee good strength of the implant, and at the same time a sufficiently large threaded periphery is obtained for the implant. This geometry of the bone-chip recesses, cutting edges and body can be obtained by milling with a so-called

dovetail cutter which has rounded corners. The bone-chip recesses can be given adequate volume, i.e. the volume can be made so great that the detached bone is accommodated without excessive compression, which can give rise to friction between fixture and surrounding bone tissue upon insertion or screwing. The design also means that clamping tendencies between the fixture/implant and the bone tissue can be minimized.

10 DESCRIPTION OF THE FIGURES

A presently proposed embodiment of an implant according to the invention will be described below with reference to the attached drawings, in which:

- 15 Figure 1 shows a side view of the implant,
 Figure 2 shows, in two cross sections B-B and C-C, a thread with reduced material or with material removed, and its remaining thread parts and specific cutting edge arrangement,
20 Figure 3 shows an end view of the implant according to Figure 1, and
 Figure 4 shows the longitudinal section A-A according to Figure 3.

25 DETAILED EMBODIMENT

- Figure 1 shows a side view of an implant which has a cylindrical threaded part and a front, cone-shaped portion with materially reduced threads. Figure
30 2 shows the cross sections B-B and C-C through the materially reduced threads according to Figure 1. According to Figure 2 and the cross section C-C, a thread with material reduction or material removed is shown with its remaining thread parts 1, 2 or 3 which
35 in this case are three in number. Between the thread parts there are spaces 4, 5, 6 which accommodate detached bone tissue. In this illustrative embodiment, the thread parts and the spaces are essentially uniformly distributed about the circumference of the

implant. Another pattern of distribution and another number of spaces are possible. The circumferential direction of the implant is indicated by 7 and the implant axis at right angles to the plane of the figure is indicated by 8.

The thread parts are provided with cutting edges 1a, 2a and 3a which cooperate with or cut into bone tissue when the implant is being threaded into the bone in the circumferential direction 7. A characteristic feature of the cutting function is that the cutting edges are designed with points or parts 1b, 2b, 3b. The thread parts also have parts 1c, 2c and 3c which extend along the full radius R or along the circumferential direction 7 and which define the thread diameter in the bone produced with the thread in question. The rear sides of the thread parts are indicated by 1d, 2d and 3d.

To form a cutting edge with cutting angle (or chip angle) α , the cutting edge extends in relation to the actual radius r at the said angle α which can be chosen at about 20° or within the range of 15-40°. At its inner parts, the cutting edge on a first thread part, for example thread part 3, merges into the rear side, for example the rear side 1d, of an adjoining thread part, for example thread part 1, via a radius-shaped or curved transition part 9 which has a certain length at right angles to the plane of the figure. A radius for the curved part is indicated by r'. One or more of the remaining thread parts can have a relief edge 2e, 3e, behind its circular part 2c and 3c, respectively.

Figure 2 shows an angle β between cutting and rear edges of successive thread parts, as viewed in the direction of rotation 7. In this illustrative embodiment, the angle β must be about 70°, and it can be of the same size or different sizes. A relief angle γ between the circular part 3c and the relief surface 3e is chosen at 5-10°.

In Figure 1, the reduced thread shown in cross section in Figure 1 is indicated by 10. The positions of the spaces 4 and 5 can also be seen, the remaining thread part between these two spaces being indicated by 2. The implant or the fixture has a cylindrical part 11 with non-reduced threads and a front cone-shaped portion 12 with materially reduced threads. The impressions or recesses have been formed by material reduction in the said threads and in the body of the implant. The free end of the implant, which is essentially straight and chosen at right angles in relation to the longitudinal axis of the implant, is indicated by 13. The upper part of the implant is indicated by 14. As can be seen from the figure, the relief edge 2e of the remaining thread part 2 consists of two essentially plane relief surfaces 2e' and 2e'' which form an obtuse angle with each other. This is best seen from the cross section B-B in Figure 2, where respective relief surfaces have been indicated.

In the end view in Figure 3, the surface 13 and the lower edge of the spaces 4 and 5 are shown. A longitudinal section A-A through the longitudinal axis of the implant is shown in Figure 4 below.

In Figure 4, the body of the implant is indicated by 15. The cone-shaped portion (or point) 12 is designed with a point angle δ which in this case is up to about 10° . The bone-chip recesses or spaces 4, 5 and 6 (see also Figure 1) are located in the cone-shaped portion 12 and continue partially into the cylindrical portion. By means of the above, non-axially arranged cutting edges are obtained via the reduced threads overlying one another. A materially reduced thread must have at least one thread part, preferably at least two thread parts, with cutting edges which reach the circumference of the thread in question. On the cone-shape portion 12, the cutting edge in this case has three thread parts 11, 16, 17 which extend to the full radius, for example r in Figure 1. For other

The implant can be provided with one, two or more thread leads or spirals. The spirals can extend

10 different thread number, or vice versa.

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